

Parasternal electromyography to determine the relationship between patient-ventilator asynchrony and nocturnal gas exchange during home mechanical ventilation set-up

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ABSTRACT

Introduction Patient-ventilator asynchrony (PVA) can adversely affect the successful initiation of non-invasive home mechanical ventilation (HMV). The aim of this observational study was to quantify the prevalence of PVA during initiation of HMV and to determine the relationship between PVA and nocturnal gas exchange.

Method Type and frequency of PVA were measured by surface parasternal intercostal muscle electromyography, thoracoabdominal plethysmography and mask pressure during initiation of HMV. Severe PVA was defined, as previously, as asynchrony affecting $\geq 10\%$ of breaths.

Results 28 patients (18 male) were enrolled aged 61 ± 15 years and with a body mass index of 35 ± 9 kg/m². Underlying diagnoses were neuromuscular disease with or without chest wall disease (n=6), obesity related chronic respiratory failure (n=12) and COPD (n=10). PVA was observed in all patients with 79% of patients demonstrating severe PVA. Triggering asynchrony was most frequent, observed in 24% (IQR: 11–36%) of breaths, with ineffective efforts accounting for 16% (IQR: 4–24%). PVA types were similar between disease groups, with the exception of auto-triggering, which was higher in patients with COPD (12% (IQR: 6–26%)). There was no correlation observed between PVA and time spent with oxygen saturations $\leq 90\%$, mean oxygen saturations or transcutaneous carbon dioxide levels during overnight ventilation.

Conclusions Severe PVA was identified in the majority of patients, irrespective of pathophysiological disease state. This was not associated with ineffective ventilation as evidenced by gas exchange.

INTRODUCTION

A European survey performed in 2005 reported that almost 22 000 patients with chronic respiratory failure were receiving home mechanical ventilation (HMV) with either non-invasive or invasive ventilation.¹ Despite the clinical benefits, a significant proportion of patients are unable to adhere to their HMV prescription.² Certain factors affecting adherence to HMV are difficult to modify, such as mask claustrophobia, but the clinical set-up of non-invasive ventilation (NIV) is operator-dependent

Key messages

What is the key question?

- To quantify the prevalence of patient-ventilator asynchrony (PVA) during home non-invasive ventilation set-up and to determine the relationship between PVA and nocturnal gas exchange?

What is the bottom line?

- PVA, measured using parasternal electromyography, is a very frequent event and, in contrast to current opinion, this study has shown that PVA was not associated with an adverse impact on nocturnal gas exchange.

Why read on?

- This physiological study of overnight set-up of non-invasive ventilation in patients with chronic respiratory failure using surface parasternal electromyography provides a comprehensive assessment of the type and frequency of PVA encountered when initiating home non-invasive ventilation.

and indeed could be enhanced if patient-ventilator synchrony were achieved.

Patient-ventilator asynchrony (PVA) describes the poor interaction between the patient and the ventilator and is the consequence of the respiratory muscle activity of the patient being opposed to the action of the ventilator. These are, in general, grouped as triggering and cycling PVA. PVA adversely affects respiratory muscle unloading during mechanical ventilation,^{3–4} which is reported from previous studies to negatively impact on the nocturnal gas exchange and sleep quality.^{5–8} Furthermore, asynchronous breaths have previously been observed to have unfavourable clinical consequences including dyspnoea perception,^{9–13} patient discomfort and intolerance^{14–15} and reduced adherence to NIV.¹⁶ Previous studies have reported that PVA can have an adverse clinical impact if greater than 10% of the breaths are asynchronous,^{14–17–18} albeit a minimal clinically important difference



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with non-invasive ventilator support has yet to be reported. Furthermore, there are limited data on the type and prevalence of asynchronous events during NIV.

More recently, the surface parasternal electromyogram (sEMGpara) has been used for the non-invasive measurement of neural respiratory drive in acute and stable settings, including overnight measurements during sleep in patients with chronic respiratory disease.^{11–13 19} As PVA describes the coordination between the respiratory effort of the patient and the mechanical breaths delivered by the ventilator, a real-time measurement of the relationship between neural respiratory drive during inspiration and the timing of ventilator pressurisation is required. We hypothesised, using this novel comparative technique, that we could quantify the type and prevalence of PVA in patients with chronic respiratory failure secondary to restrictive and obstructive lung disease during overnight HMV set-up and, in addition, investigated the relationship between PVA and nocturnal gas exchange.

METHODS

Patients

Patients were referred to a tertiary centre for management of chronic respiratory failure between September 2010 and December 2012. All participants provided written informed consent at enrolment.

Definition of PVA

Following a comprehensive review of the literature (see online supplementary material for search terms) and discussions with international HMV experts, a group consensus was reached in defining the types of PVA. We divided PVA into triggering and cycling asynchronies and used these as reference for this study.^{14 17 20 21} The triggering asynchronies included ineffective efforts, auto-triggering, double triggering and multiple triggering and the cycling asynchronies included premature expiratory cycling, delayed expiratory cycling and autocycling. The definitions of the specific types of triggering and cycling PVA, with worked examples, are described in detail in the online supplementary appendix E1 and figure E1–E8.

NIV set-up and measurements

All patients were admitted for nocturnal set-up and titration of NIV (NIPPY3+ ventilator; B&D Electromedical, Stratford-upon-Avon, UK) according to standard clinical protocols depending upon their underlying pathophysiological condition (see online supplementary appendix E2a–E2c) in a pressure support mode with a fixed backup rate set at two breaths below the resting breathing rate, as previously reported.²² Measurement of sEMGpara was employed as a physiological biomarker to mark the onset and level of neural respiratory drive.^{11–13} The second intercostal space was identified using bony landmarks and skin was prepared with EMG contact gel (Nuprep, DO Weaver and Co, Colorado, USA). Wet gel electrodes (Neuroline 720, Ambu, Ballerup, Denmark) were placed adjacent to the sternal edge in the second intercostal spaces. The sEMGpara signal was amplified, processed, filtered and analysed in standard conditions according to the methods previously described¹² (see online supplementary material for details). sEMGpara recordings were performed with the patient lying in bed in their preferred sleeping position and acquired throughout the whole night. Respiratory inductance plethysmography (Respirtrace, SensorMedics, Miami Beach, Florida) was concurrently used to measure chest wall excursion and abdominal wall excursion to assist the analyser to gait against postural sEMGpara movement artefacts. Patients underwent overnight

measurements of mask pressure using a standard pressure transducer with a range between +200 cm H₂O and –200 cm H₂O (GM Instruments, Kilwinning, UK). Transcutaneous oximetry (SpO₂) and capnometry (TcCO₂) were calibrated to arterial carbon dioxide levels and measured using a TOSCA 500 monitor (Radiometer Medical, Copenhagen, Denmark). All data were analysed using LabChart V7.3.7 (AD Instruments, Chalgrove, UK) (figure 1).

Type and frequency of PVA

Manual recording analysis was performed in 10 min epochs throughout the whole night of NIV use, with the final 2 min of each epoch analysed for type and frequency of PVA according to the a priori definitions (see online supplementary appendix E1 and figures E1–E8). The 1st hour of recording and movement artefacts were discarded with the nearest artefact-free 2 min epoch analysed instead. The proportion of PVA was calculated as the number of asynchronous breaths divided by the total number of breaths (requested and delivered) multiplied by 100, as described by Thille *et al.*¹⁷

Ventilator set-up

Every ventilator-delivered breath in the 10 min epochs was analysed as a triggered pressure support delivered breath, an inappropriate auto-triggered delivered breath or an appropriate pressure control delivered ‘backup’ breath (identified by rate and set inspiratory time). All ventilators were set in pressure support (S/T) mode with a backup rate set 2 below the resting respiratory rate. Comparative analysis of the PVA frequency when patients received ≥70% breaths from either pressure supported (patient triggered) or pressure controlled (ventilator delivered) ventilation was performed.

Inter-rater reliability of PVA

Two assessors (authors MR and SM) were blinded and independently scored 10 randomly selected 1 h sections of recorded data from 10 patients. Asynchronous events were manually assessed according to the a priori definitions (see online supplementary appendix E1 and figures E1–E8).

Statistical analysis

Patient demographic data and the type of ventilator-delivered breaths are expressed as mean±SD, and a one-way analysis of variance and pairwise tests with a Bonferroni correction were used to compare patient groups. Data that was not normally distributed are reported as median values with IQRs. Comparative analysis of the differences in the ventilator set-up parameters and frequency of the types of PVA between the patient groups were made using the Kruskal-Wallis test. Comparative analysis between the number of pressure support breaths and pressure control breaths delivered by the ventilator were assessed using a Mann-Whitney U test. Simple rank regressions were performed to assess the strength of the relationship with PVA and nocturnal gas exchange. Statistical analyses were conducted using SPSS (V.19, IBM Corporation, USA) and GraphPad (Prism 6, GraphPad software, USA). A p value <0.05 was taken to represent statistical significance. Further details of the statistical analyses performed are placed in the online supplementary material.

RESULTS

Type and frequency of PVA

Patient demographics

All 28 patients (18 male) approached were recruited at an age of 61±15 years, a body mass index (BMI) of 35±9 kg/m², an

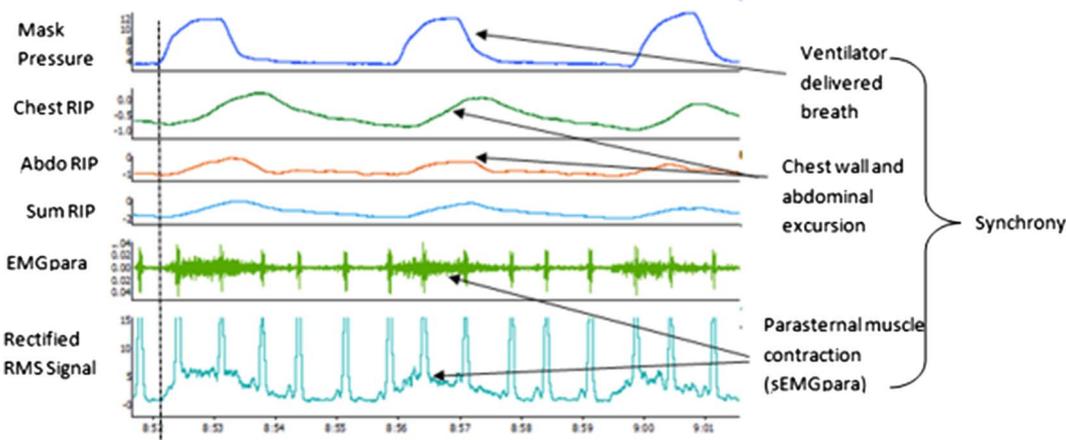


Figure 1 An example of satisfactory patient ventilator synchrony. Chest RIP, chest wall respiratory inductance plethysmography; Abdo RIP, abdominal respiratory inductance plethysmography; Sum RIP, combined chest and abdominal inductance plethysmography; EMGpara, parasternal intercostal electromyography; RMS, rectified root mean square of parasternal electromyography signal.

FEV₁ of 1.1±0.5 L and an FVC of 1.6±0.7 L. Six patients had neuromuscular disease with or without chest wall disease (NMD-CWD), 12 had obesity related respiratory failure (ORRF; BMI ≥30 kg/m² with a daytime pCO₂ ≥6 kPa in the absence of any other cause) and 10 had COPD. Baseline demographic data are presented in table 1.

There were no differences in the age of the patients between patient groups and all patients had a BMI in the ‘overweight’ or ‘obese’ range. Four of the 10 patients with COPD had concurrent upper airways obstruction defined by a baseline oxygen desaturation index below 4% above 10 events per hour reflecting increasing trends of obesity in the UK. Patients with COPD were also more hypoxic and hypercapnic than the patients with NMD-CWD at baseline (arterial oxygen level 7.6±1.4 kPa vs 9.2±0.6 kPa; p<0.04 and arterial carbon dioxide level 7.9±1.0 kPa vs 6.6±1.0 kPa; p<0.03, respectively).

Ventilator set-up

There was no difference between the number of pressure supported and pressure controlled breaths delivered overnight across the whole group (44±26% vs 41±31%; p=0.7). Individual disease groups exhibited different interactions with the ventilator in terms of triggering the ventilator (table 2). Furthermore, as expected, those patients from the cohort that received over 70% pressure support breaths (n=6) had a higher

percentage of asynchronous breaths overnight than those patients that received over 70% pressure control breaths (n=5) (30% (27–38%) vs 9% (1–10%), respectively; p<0.01). Patients that received more than 70% pressure support breaths demonstrated higher levels of ineffective efforts than those with more than 70% of pressure control delivered breaths (15% (10–20%) vs 1% (0–2%); p<0.01).

Further details of the ventilator settings used between patient groups is available in the online supplementary material results section.

Patient-ventilator asynchrony

A total of 27 637 breaths were analysed from the 2 min epochs of overnight data recorded. Combined triggering and cycling PVA had an overall prevalence of 28±19% across all patients studied. Indeed, 79% of patients were observed to have an asynchrony index greater than 10% of breaths (range 11–63%). Ineffective efforts were the most common PVA observed in 89.3% of patients and accounted for 15±11% of breaths. Other PVA including auto-triggering, delayed expiratory cycling and premature cycling were observed in 85.7%, 67.9% and 85.7% of patients but with only 3% (0–9%), 1% (0–5%) and 1% (0–2%) of the total breaths affected, respectively. Double triggering, multiple triggering and autocycling were less frequent affecting 53.6%, 35.7% and 46.4% of patients,

Table 1 Comparison of baseline patient demographics by disease group

Demographics	COPD (n=10)	NMD-CWD (n=6)	ORRF (n=12)	p Value
Age (years)	66±10	58±22	59±16	0.54
BMI (kg/m ²)	30.0±5.2	27.2±5.3	43.0±4.8	<0.0001*
FEV ₁ (% predicted)	31.1±11.3	32.7±11.3	52.5±20.2	<0.01*
FVC (% predicted)	52.4±9.7	30.5±10.7	55.6±19.0	<0.01*
FEV ₁ /FVC (% ratio)	45.8±11.0	85.4±3.6	81.2±8.5	<0.001*
PaO ₂ (kPa)	7.6±1.4	9.2±0.6	8.3±1.0	<0.03*
PaCO ₂ (kPa)	7.9±1.0	6.6±1.0	7.1±0.9	<0.04*
HCO ₃ ⁻ (mmol/l)	33.5±3.2	30.8±3.8	31.5±3.8	0.28

*A one-way analysis of variance was used to compare the demographics between disease groups, p value <0.05 was taken to represent statistical significance. BMI, body mass index; HCO₃⁻, serum bicarbonate level; NMD-CWD, neuromuscular disease with or without chest wall disease; ORRF, obesity related respiratory failure; PaCO₂, arterial carbon dioxide level; PaO₂, arterial oxygen level.

Table 2 Comparison of non-invasive ventilator set-up by disease group

Ventilator parameters	COPD	NMD-CWD	ORRF	p Value
IPAP (cmH ₂ O)	18 (18–25)	15 (14–21)	20 (18–28)	0.1
EPAP (cmH ₂ O)	4 (3–7)	3 (3–4)	9 (8–12)	<0.001*
Backup rate (breaths/min)	14 (11–14)	14 (14–14)	14 (13–16)	0.3
% Pressure support breaths	60±25	34±24	36±56	0.06
% Pressure control breaths	25±30	47±24	51±31	0.09
% Ineffective efforts	15±11	19±13	13±10	0.4
% Total patient ventilator asynchrony	43±29	29±19	24±17	0.3

*A Kruskal-Wallis test was used to compare the ventilator parameters between disease groups, p value <0.05 was taken to represent statistical significance. All results expressed as median and IQR.

Pressure support breaths and pressure control breaths represent the ventilator delivered breaths, ineffective efforts represent the patient demanded breaths that were not met, combined they represent all breaths (requested and delivered).

EPAP, expiratory positive airway pressure; IPAP, inspiratory positive airway pressure; NMD-CWD, neuromuscular disease with or without chest wall disease; ORRF, obesity related respiratory failure.

respectively, and these accounted for 0% (0–1%), 0% (0–0%) and 0% (0–0%) of breaths, respectively.

Comparison of PVA by disease category

Across all groups, triggering asynchronies were greater than cycling asynchronies with 24% (11–36%) of total breaths demonstrating triggering asynchronies and 5% (1–8%) of total breaths demonstrating cycling asynchronies in all patients ($p < 0.0001$). PVA, including triggering asynchronies (table 3) and cycling asynchronies (table 4), was observed in all patient groups ranging from 33% (19–78%) of total breaths in patients with COPD, 31% (10–45%) of breaths in patients with NMD-CWD and 29% (9–38%) of breaths in patients with ORRF ($p = 0.3$).

The most frequent asynchrony was ineffective effort, albeit there was no difference across the disease groups ($p = 0.4$). The only difference observed between patients with COPD, NMD-CWD and ORRF was in auto-triggering, affecting 12% (6–36%), 6% (1–8%) and 2% (0–6%) of breaths, respectively ($p = 0.04$).

Overnight gas exchange

Overnight gas exchange was assessed using nocturnal oximetry and capnography, which has been shown to accurately monitor and track changes in nocturnal gas exchange in patients receiving NIV.²³ Patients demonstrated nocturnal hypoventilation with a mean SpO₂ of 91±7% and TcCO₂ of 7.8±1.3 kPa during the first night of NIV set-up without the use of supplemental oxygen. Of the overnight total analysis time 35±33% was spent with oxygen saturations below 90% (TBI90) in a subset of 16 patients. Patients with ORRF were more hypoxic overnight than patients with NMD-CWD (SpO₂ of 88±8% vs 96±4%; $p = 0.02$). There were no associations observed between total

overnight PVA events and nocturnal SpO₂ ($r^2 = 0.08$; $p = 0.16$) and TcCO₂ ($r^2 < 0.001$; $p = 0.94$). Furthermore, there was no relationship observed between nocturnal SpO₂ and TcCO₂ and the percentage of ineffective efforts ($r^2 = 0.04$; $p = 0.32$ and $r^2 = -0.04$; $p = 0.32$, respectively). Finally, there was no association observed between the TBI90 and the percentage of asynchronous breaths or ineffective efforts ($r^2 = -0.02$; $p = 0.12$ and $r^2 = -0.08$; $p = 0.36$, respectively) in the subset of patients examined.

Inter-rater reliability of assessment of PVA

Ten patients (four COPD, four ORRF and two NMD-CWD) were included in this substudy. A total of 4603 breaths were analysed by two independent scorers with PVA reported in 812 (35%) and 891 (39%) breaths, respectively. The intraclass correlation coefficient between the scorers was 0.84 (0.74–0.90). The predominant asynchrony reported was ineffective efforts, for which there was the closest interobserver agreement with an intraclass correlation coefficient of 0.94 (0.79–0.99). The agreement for triggering and cycling PVA are shown in tables 5 and 6. The lowest agreement was observed in the autocycling asynchrony (0.22; -0.54 – 0.74), albeit this had a very low frequency and was observed in <1% of the total breaths analysed.

DISCUSSION

This is the first study to report a comprehensive overnight assessment of PVA during first night initiation of non-invasive ventilation. Previous studies have either been daytime or overnight studies in patients established on HMV and these studies lacked description of all types and frequencies of PVA.^{6–8 14 17 24} Neural respiratory drive, as measured from surface electromyogram of the second intercostal parasternal muscles, combined with

Table 3 Triggering asynchrony during overnight NIV setup

% of breaths	COPD	NMD-CWD	ORRF	p Value
% Ineffective efforts	15 (6–23)	24 (5–27)	14 (2–21)	0.4
% Auto-triggering	12 (6–36)	2 (0–6)	6 (1–8)	0.04*
% Multiple triggering	0 (0–0)	0 (0–0)	0 (0–0)	0.1
% Double triggering	0 (0–1)	0 (0–3)	0 (0–1)	0.6
% Total triggering asynchrony	26 (13–66)	27 (7–39)	21 (9–31)	0.3

A Kruskal-Wallis test was used to compare patient-ventilator asynchrony between disease groups, p value <0.05 was taken to represent statistical significance. NMD-CWD, neuromuscular disease with or without chest wall disease; ORRF, obesity related respiratory failure.

Table 4 Cycling asynchrony during overnight NIV setup

% of breaths	COPD	NMD-CWD	ORRF	p Value
% Premature expiratory cycling	1 (0–4)	1 (0–4)	1 (0–2)	0.9
% Delayed expiratory cycling	2 (0–7)	2 (0–5)	0 (0–3)	0.5
% Auto-cycling	1 (0–4)	0 (0–0)	0 (0–0)	0.2
% Total cycling asynchrony	7 (4–10)	4 (3–6)	3 (1–7)	0.2

A Kruskal-Wallis test was used to compare patient-ventilator asynchrony between disease groups, p value <0.05 was taken to represent statistical significance. NMD-CWD, neuromuscular disease with or without chest wall disease; ORRF, obesity related respiratory failure.

Table 5 Agreement of triggering asynchrony between two independent scorers

Type of asynchrony	Scorer 1 n (% breaths)	Scorer 2 n (% breaths)	ICC (95% CI)	Bland-Altman analysis bias (95% limits of agreement)
Ineffective efforts	484 (21%)	466 (21%)	0.94 (0.79 to 0.99)	1.8 (−30.1 to 33.7)
Auto-triggering	164 (7%)	231 (10%)	0.77 (0.19 to 0.94)	−6.7 (−25.4 to 12.0)
Double triggering	22 (<1%)	11 (<1%)	0.67 (0.11 to 0.91)	1.1 (−1.9 to 4.1)
Multiple triggering	4 (<1%)	4 (<1%)	1.00	0.0 (0.0 to 0.0)

ICC, intraclass correlation coefficient.

measurements of thoracoabdominal motion and mask pressure has been shown to be accurate and reliable in assessing trigger and cycling PVA during NIV. Importantly, we have detailed the high prevalence of PVA during initiation of HMV in patients with stable chronic respiratory failure and shown that up to a third of the breaths were asynchronous during the initiation of HMV, irrespective of the underlying disease pathology. Triggering asynchrony rather than cycling asynchrony was shown to be the most frequent PVA. Of major relevance to the clinician, there was no relationship between PVA and overnight gas exchange, which implies that the adequate delivery of ventilation during HMV set-up, based on the frequency and level of airway pressurisation, is of greater importance to optimise adequacy of gas exchange, rather than optimising PVA.

Critique of the method

We acknowledge that sEMGpara has recognised limitations, including postural artefacts and potential contamination of the signal from other chest wall muscles.²⁵ Needle electrodes could have been used to directly isolate parasternal muscle activity, but this is unsuitable for overnight monitoring in the clinical setting and may risk pneumothorax.²⁶ Alternatively, an oesophageal electrode may be used to monitor the diaphragm electromyogram, but again this is poorly tolerated in stable patients and the use of such an invasive technique in clinical practice for overnight studies is wholly challenging.

Although patients in this study were directly observed to be sleeping overnight by the research team, this was not confirmed through full montage polysomnography (PSG) and the authors acknowledge this. However, PSG is not routinely used in clinical practice for HMV initiation in the UK, and indeed recent European guidance has recommended using PSG only when simple tools to optimise NIV set-up have failed.²⁷

For practical reasons, and based on our previous daytime laboratory studies,²⁸ mask leak was not assessed in this overnight study as the burden of the pneumotach in the experimental mask-ventilator circuit actually contributed to greater air leak and consequently this would have increased PVA. Indeed, air leak induced PVA would have been a major confounder during the overnight studies.^{7 14}

Physiological observations

Prevalence of PVA

By using a non-invasive approach to monitor physiological variables over the whole night, we have demonstrated that the prevalence of PVA, irrespective of the underlying disease pathology, was substantially greater than that previously reported.^{6–8 14 17 24} Up to a third of all breaths, during NIV set-up, were asynchronous. PVA was demonstrated in all patients studied, compared with previous studies which have reported a PVA prevalence of 0–77% of patients.^{5 24} These current data reflect the enhanced details of this advanced monitoring technique.

Triggering asynchrony

An ineffective effort was the most frequent type of PVA observed during the initiation of HMV. Similar to recent work by Carlucci *et al*,¹⁶ there was no difference in the prevalence of this asynchrony between the patient groups. Interestingly, auto-triggered breaths affected most patients, but the frequency of these events was very low. Furthermore, auto-triggering was most commonly observed in patients with COPD and this is likely to be a consequence of mask leak, as previously reported.²⁴ In addition, patients with COPD have an increased airway secretion load and this has previously been demonstrated to contribute to auto-triggering of the ventilator.²⁹ Despite the observation that double triggering and multiple triggering were demonstrated in up to 50% of patients, the frequency of this PVA in the current study was very low and therefore unlikely to have clinical relevance during the initiation of HMV. Furthermore, cycling asynchrony was observed to be infrequent.

Asynchrony and overnight gas exchange

Despite higher levels of asynchrony observed in our cohort, there was no demonstrable effect on overnight gas exchange. This is in contrast to previous data suggesting that ineffective efforts are associated with overnight oxygen desaturation.⁶ This may, in part, be explained by the ventilator backup rate in the current study, supported by the proportion of pressure controlled breaths delivered, which was up to 46%, depending on the patient group. The study by Fanfulla *et al*⁶ was performed

Table 6 Agreement of cycling asynchrony between two scorers

Type of asynchrony	Scorer 1 n (% breaths)	Scorer 2 n (% breaths)	ICC (95% CI)	Bland-Altman analysis bias (95% limits of agreement)
Premature cycling	88 (4%)	124 (5%)	0.73 (0.26 to 0.92)	−3.6 (−18.7 to 11.5)
Extended cycling	45 (2%)	50 (2%)	0.76 (0.31 to 0.93)	−0.5 (−8.6 to 7.6)
Auto-cycling cycling	5 (<1%)	5 (<1%)	0.22 (−0.54 to 0.74)	0.0 (−2.3 to 2.3)

A total of 4603 breaths were analysed with patient ventilator asynchrony reported in 812 and 891 breaths by scorer 1 and scorer 2, respectively. ICC, intraclass correlation coefficient.

in patients already established on HMV and the study used low level pressure support and, rather unusually for patients with NMD, there was no back-up rate applied. This would not be the current clinical approach, based on the current evidence, which supports the use of a mandatory backup rate in patients with NMD,³⁰ patients with ORRF^{22, 31} and patients with COPD.³² The current data have demonstrated that optimal set-up of the inspiratory positive airway pressure, the expiratory positive airway pressure and the backup rate is more important, in terms of control of gas exchange, than PVA.

Clinical implications

Previous work has shown that clinician scoring of PVA through non-invasive measurements of ventilator flow and pressure waveform fail to report up to two-thirds of events.³³ Other studies using automated algorithms to detect asynchrony have improved frequency detection but have been limited in detailing the type of PVA.^{34, 35} However, the current study has demonstrated adequate levels of agreement between two independent observers comprehensively reporting triggering and cycling asynchrony. This non-invasive technique is potentially suitable to assist the clinician in optimising the ventilator settings during NIV set-up with real-time visual feedback of the impact of the ventilator changes at the bedside. For example, this novel approach can determine the physiological cause of the double triggered breath, where other methods would fail. This event can occur due to the first ventilator-delivered breath prematurely cycling out and the second ventilator-delivered breath appropriately triggered by the ongoing inspiratory effort of the patient, evidenced by increasing amplitude of the neural respiratory drive (figure 2A). Alternatively, this event can reflect

inappropriate auto-triggering of the second breath such that there is no increase in the neural respiratory drive observed (figure 2B). The addition of sEMGpara, as a marker of neural inspiratory drive, assists the scorer in distinguishing between the two phenomena and enables appropriate adjustment of the ventilator.

Previous work has suggested that PVA, in particular ineffective efforts, has an adverse effect of overnight gas exchange.⁶ However, the data from the current study have shown that during NIV set-up PVA has limited impact on gas exchange, in terms of SpO₂, TBI90 and TcCO₂ levels. Even high levels of asynchrony, irrespective of the type, had limited effect on overnight gas exchange, suggesting that adequate ventilation, based on inspiratory and expiratory positive airway pressures and backup rate, will enhance gas exchange irrespective of patient-ventilator synchronisation. Furthermore, the current study indicates that optimising the ventilator settings so that the patient receives a greater proportion of pressure controlled breaths than pressure supported breaths may confer a benefit in reducing levels of PVA and, in particular, ineffective efforts. This is supported by previous data published by our own group on morbidly obese patients²² and it may explain, in part, the benefits of a high intensity non-invasive positive pressure ventilation in stable COPD.³² Controlled data detailing the effect of PVA on patient-centred outcomes, such as sleep quality, daytime symptoms and health related quality of life, will be reported in the future (<http://www.clinicaltrials.gov> NCT01371149).

CONCLUSION

Physiological measurements combining neural respiratory drive, thoracoabdominal movement and mask pressure monitoring

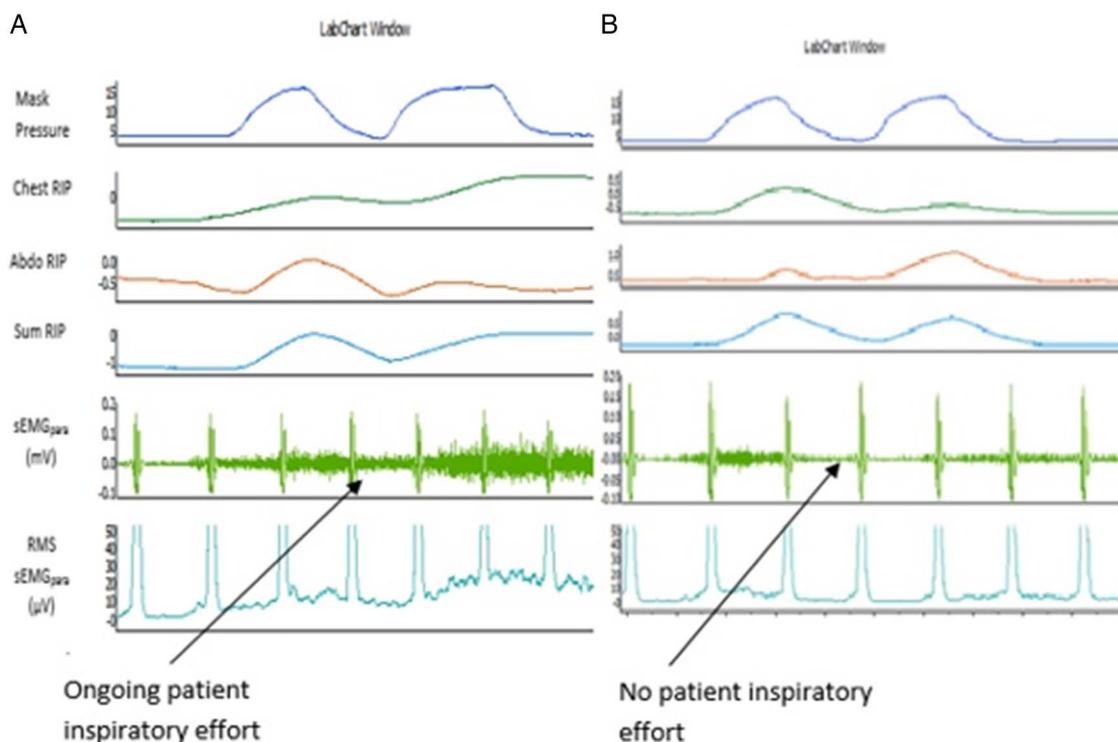


Figure 2 'Double triggering' was confirmed with the addition of second intercostal space electromyography to the mask pressure measurement and respiratory inductance plethysmography. (A) shows a prematurely cycled breath with ongoing patient inspiratory effort to trigger a second ventilator-delivered breath and (B) shows a patient-triggered breath followed by a nonpatient-triggered breath, which by definition is an 'auto-triggered' breath. Chest RIP, chest wall respiratory inductance plethysmography; Abdo RIP, abdominal respiratory inductance plethysmography; Sum RIP, combined chest and abdominal inductance plethysmography; EMGpara, parasternal intercostal electromyography; RMS, rectified root mean square of parasternal electromyography signal.

have been shown as a reliable technique to non-invasively score the type and frequency of PVA observed during initiation of NIV in patients with chronic respiratory failure. Using this technique, we have demonstrated high levels of asynchrony, irrespective of the underlying aetiology of chronic respiratory failure, with triggering asynchrony reported as the most frequent type of asynchrony observed. Of major clinical relevance, there was no correlation between the type and frequency of asynchrony and overnight gas exchange during inpatient NIV set-up.

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REFERENCES

- Lloyd-Owen SJ, Donaldson GC, Ambrosino N, *et al.* Patterns of home mechanical ventilation use in Europe: results from the Eurovent survey. *Eur Respir J* 2005;25:1025–31.
- Criner GJ, Brennan K, Travaline JM, *et al.* Efficacy and compliance with noninvasive positive pressure ventilation in patients with chronic respiratory failure. *Chest* 1999;116:667–75.
- Leung P, Jubran A, Tobin MJ. Comparison of assisted ventilator modes on triggering, patient effort, and dyspnea. *Am J Respir Crit Care Med* 1997;155:1940–8.
- Nava S, Bruschi C, Fracchia C, *et al.* Patient-ventilator interaction and inspiratory effort during pressure support ventilation in patients with different pathologies. *Eur Respir J* 1997;10:177–83.
- Fanfulla F, Delmastro M, Berardinelli A, *et al.* Effects of different ventilator settings on sleep and inspiratory effort in patients with neuromuscular disease. *Am J Respir Crit Care Med* 2005;172:619–24.
- Fanfulla F, Taurino AE, Lupo ND, *et al.* Effect of sleep on patient/ventilator asynchrony in patients undergoing chronic non-invasive mechanical ventilation. *Respir Med* 2007;101:1702–7.
- Crescimanno G, Canino M, Marrone O. Asynchronies and sleep disruption in neuromuscular patients under home noninvasive ventilation. *Respir Med* 2012;106:1478–85.
- Guo YF, Sforza E, Janssens JP. Respiratory patterns during sleep in obesity-hypoventilation patients treated with nocturnal pressure support: a preliminary report. *CHEST* 2007;131:1090–9.
- Adler D, Perrig S, Takahashi H, *et al.* Polysomnography in stable COPD under non-invasive ventilation to reduce patient-ventilator asynchrony and morning breathlessness. *Sleep Breath* 2012;16:1081–90.
- Jolley CJ, Moxham J. A physiological model of patient-reported breathlessness during daily activities in COPD. *Eur Respir Rev* 2009;18:66–79.
- Reilly CC, Ward K, Jolley CJ, *et al.* Neural respiratory drive, pulmonary mechanics and breathlessness in patients with cystic fibrosis. *Thorax* 2011;66:240–6.
- Murphy PB, Kumar A, Reilly C, *et al.* Neural respiratory drive as a physiological biomarker to monitor change during acute exacerbations of COPD. *Thorax* 2011;66:602–8.
- Steier J, Jolley CJ, Polkey MI, *et al.* Nocturnal asthma monitoring by chest wall electromyography. *Thorax* 2011;66:609–14.
- Vignaux L, Vargas F, Roeseler J, *et al.* Patient-ventilator asynchrony during non-invasive ventilation for acute respiratory failure: a multicenter study. *Intensive Care Med* 2009;35:840–6.
- Vitacca M, Bianchi L, Zanotti E, *et al.* Assessment of physiologic variables and subjective comfort under different levels of pressure support ventilation. *Chest* 2004;126:851–9.
- Carlucci A, Pisani L, Ceriana P, *et al.* Patient-ventilator asynchronies: may the respiratory mechanics play a role? *Crit Care* 2013;17:R54.
- Thille AW, Rodriguez P, Cabello B, *et al.* Patient-ventilator asynchrony during assisted mechanical ventilation. *Intensive Care Med* 2006;32:1515–22.
- de Wit M, Miller KB, Green DA, *et al.* Ineffective triggering predicts increased duration of mechanical ventilation. *Crit Care Med* 2009;37:2740–5.
- Jolley CJ, Luo YM, Steier J, *et al.* Neural respiratory drive in healthy subjects and in COPD. *Eur Respir J* 2009;33:289–97.
- Piquilloud L, Vignaux L, Bialais E, *et al.* Neurally adjusted ventilatory assist improves patient-ventilator interaction. *Intensive Care Med* 2011;37:263–71.
- Vignaux L, Grazioli S, Piquilloud L, *et al.* Patient-ventilator asynchrony during noninvasive pressure support ventilation and neurally adjusted ventilatory assist in infants and children. *Pediatr Crit Care Med* 2013;14:e357–64.
- Murphy PB, Davidson C, Hind MD, *et al.* Volume targeted versus pressure support non-invasive ventilation in patients with super obesity and chronic respiratory failure: a randomised controlled trial. *Thorax* 2012;67:727–34.
- Storre JH, Magnet FS, Dreher M, *et al.* Transcutaneous monitoring as a replacement for arterial PCO₂ monitoring during nocturnal non-invasive ventilation. *Respir Med* 2011;105:143–50.
- Carteaux G, Lyazidi A, Cordoba-Izquierdo A, *et al.* Patient-ventilator asynchrony during noninvasive ventilation: a bench and clinical study. *Chest* 2012;142:367–76.
- Luo YM, Moxham J, Polkey MI. Diaphragm electromyography using an oesophageal catheter: current concepts. *Clin Sci* 2008;115:233–44.
- Gandevia SC, Hudson AL, Gorman RB, *et al.* Spatial distribution of inspiratory drive to the parasternal intercostal muscles in humans. *J Physiol* 2006;573(Pt 1):263–75.
- Janssens JP, Borel JC, Pepin JL, *et al.* Nocturnal monitoring of home non-invasive ventilation: the contribution of simple tools such as pulse oximetry, capnography, built-in ventilator software and autonomic markers of sleep fragmentation. *Thorax* 2011;66:438–45.
- Hart N, Hunt A, Polkey MI, *et al.* Comparison of proportional assist ventilation and pressure support ventilation in chronic respiratory failure due to neuromuscular and chest wall deformity. *Thorax* 2002;57:979–81.
- Epstein SK. How often does patient-ventilator asynchrony occur and what are the consequences? *Respir Care* 2011;56:25–38.
- Hull J, Aniapravan R, Chan E, *et al.* British Thoracic Society guideline for respiratory management of children with neuromuscular weakness. *Thorax* 2012;67(Suppl 1):i1–40.
- Contal O, Adler D, Borel JC, *et al.* Impact of different back-up respiratory rates on the efficacy of non-invasive positive pressure ventilation in obesity hypoventilation syndrome: a randomized trial. *Chest* 2013;143:37–46.
- Windisch W, Haanel M, Storre JH, *et al.* High-intensity non-invasive positive pressure ventilation for stable hypercapnic COPD. *Int J Med Sci* 2009;6:72–6.
- Colombo D, Cammarota G, Alemanni M, *et al.* Efficacy of ventilator waveforms observation in detecting patient-ventilator asynchrony. *Crit Care Med* 2011;39:2452–7.
- Mulqueeny Q, Redmond SJ, Tassaux D, *et al.* Automated detection of asynchrony in patient-ventilator interaction. *Conf Proc IEEE Eng Med Biol Soc* 2009;2009:5324–7.
- Chen CW, Lin WC, Hsu CH, *et al.* Detecting ineffective triggering in the expiratory phase in mechanically ventilated patients based on airflow flow and pressure deflection: feasibility of using a computer algorithm. *Crit Care Med* 2008;36:455–61.