The cardiorespiratory response to exercise in thoracic scoliosis

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Shneerson, J M (1978). Thorax, 33, 457–463. The cardiorespiratory response to exercise in thoracic scoliosis. Twenty-six subjects with thoracic scoliosis due to various causes have been investigated. They all performed a progressive exercise test under standardised conditions, and their maximum oxygen uptake (\(\dot{V}O_2\) max), blood gases, and ventilatory and heart rate responses were observed.

The \(\dot{V}O_2\) max was significantly below normal and was proportional to the forced expiratory volume in one second (FEV1) and maximum exercise ventilation (VE max). Exercise was limited by ventilatory factors in 80% of the subjects who exercised maximally. VE max was diminished, but the dyspnoeic index was normal. The minute ventilation (VE) at any given \(\dot{V}O_2\) was about 20% greater than normal. This hyperventilation taken with the low VE max explains why exercise is usually ventilation-limited in these subjects.

Tidal volume (VT) increased linearly with ventilation until VT max was reached. The tidal volumes at any given ventilation were less than normal, but when expressed as a percentage of vital capacity (VC) they were above normal. The heart rate increased more rapidly than normal, but this appears to be a physiological result of the small muscle mass of these subjects and not a pathological response.

Hippocrates noted that hunchbacks were “affected with difficulty of breathing.” Hutchinson (1844) showed that their vital capacity (VC) was diminished, and Anthony (1930), using a hydrogen mixing technique, showed the small total lung capacity, residual volume, and functional residual capacity. Brief accounts of the heart rate (HR) and ventilation responses to exercise were reported by Samuelsson (1950), Bergofsky et al (1959), and Włodyka and Wierusz (1974), but in each case the number of patients was small and little detail of the type of exercise was given.

Taylor et al (1963) have shown that the results of exercise tests are unreliable unless they are performed under carefully standardised conditions. Recently, exercise tests in which the work rate is progressively increased have largely taken the place of steady state tests for clinical use (Godfrey, 1974) and values for normal subjects have been obtained (eg Spiro, 1975).

In the present study the subjects exercised on a bicycle ergometer against progressively increasing loads, and their heart rate and respiratory responses have been described in detail.

Subjects and methods

Twenty-six subjects (10 male and 16 female) with thoracic scoliosis gave informed consent to be studied. Their ages ranged from 13 to 67 years (mean 28.8). The scoliosis was congenital in five, idiopathic in six, followed poliomyelitis or other neurological disease in nine, and was associated with Marfan’s syndrome in three and neurofibromatosis in three. Fifteen had previously undergone spinal fusion. None had any cardiac or respiratory disease complicating the scoliosis.

The angle of scoliosis was determined by the method of Cobb (1948). The patients were weighed and their fat free mass determined by the formula of Durnin and Womersley (1974) from the skinfold thickness over the biceps muscles. The FEV1 and vital capacity were measured with a dry spirometer (Vitalograph) and the maximum voluntary ventilation over 15 s with a low-resistance 9-litre wet spirometer (P K Morgan). The latter value was multiplied by four and converted to BTPS to give the maximum ventilatory volume MVV (l/min).
mean anthropometric and spirometric data are shown in table 1.

An arterial cannula was used to obtain blood samples for gas analysis on an IL 213 blood gas analyser. Exercise was performed while sitting on an electrically-braked ergometer (Lode). The inspiratory minute volume was measured by a Parkinson Cowan CD4 dry gas meter with an electrical output to a direct-writing ink-jet recorder (Mingograf 81) (fig 1). The gas meter was calibrated with a sinusoidal pump operating at various stroke volumes and frequencies. The gas meter was connected by wide-bore tubing to a low resistance two-way respiratory valve (P K Morgan 71522) with a dead space of 60 ml. The resistance of the system to inspiration was 0.43 cmH2O at 10 l/min and 0.95 cmH2O at 70 l/min. The expired gas passed through wide-bore connecting tubing to a mixing chamber of 7.8 l capacity containing an electrically-driven fan. A sample of the mixed expired gas was dried with magnesium perchlorate and passed through a paramagnetic Servomex OA 150 oxygen analyser and an infrared absorption CO2 analyser (URAS 4). The Servomex response was linear over the range 14–21% O2 and the URA 4 over the range 0–5% CO2. The 95% response times of both to a square wave of gas leaving the mixing chamber were four seconds. Both machines were connected electrically to the Mingograf and were re-calibrated before and after each test. Oxygen uptake was calculated using a nitrogen correction and agreed within 5% with simultaneous measurements based on chemical analyses of expired gas collected in Douglas bags.

The patients were familiarised with the apparatus on the day before the tests. They rested on the ergometer until their inspired ventilation, mixed expired gas composition, and heart rate were steady. They then began pedalling, initially at a work rate of 15 watts. The work rate was increased by 15 watts each minute and the patients were encouraged to keep exercising until limited by severe dyspnoea or tiredness, a respiratory rate above 40/min, and a pulse rate above 170/min. Twenty patients achieved maximal exercise. Exercise was considered “ventilation-limited” if it was stopped because of dyspnoea with a steady tidal volume, respiratory rate >40/min, and pulse <170 beats min⁻¹ and a rapid fall in ventilation after exercise.

The slope of the relationship between VE and HR and the VO2 was calculated from the linear part of the

Table 1 Anthropometric and spirometric data

<table>
<thead>
<tr>
<th>Group</th>
<th>Weight (kg)</th>
<th>Fat free mass (kg)</th>
<th>Height (cm)</th>
<th>Arm span (cm)</th>
<th>Angle of scoliosis (degrees)</th>
<th>FEV1 (l)</th>
<th>VC (l)</th>
<th>MVV (l min⁻¹)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Male</td>
<td>Range</td>
<td>20–74</td>
<td>19–59-9</td>
<td>123–169</td>
<td>138–192</td>
<td>20–130</td>
<td>0.50–2.85</td>
<td>0.55–2.90</td>
</tr>
<tr>
<td></td>
<td>Mean</td>
<td>50.8</td>
<td>42.1</td>
<td>155.5</td>
<td>171</td>
<td>75–4</td>
<td>1.50</td>
<td>1.69</td>
</tr>
<tr>
<td></td>
<td>SD</td>
<td>14–1</td>
<td>10.4</td>
<td>11–9</td>
<td>15–1</td>
<td>30.3</td>
<td>0.70</td>
<td>0.73</td>
</tr>
<tr>
<td>Female</td>
<td>Range</td>
<td>22.5–58</td>
<td>19.3–44.5</td>
<td>130.5–162</td>
<td>132–200</td>
<td>25–115</td>
<td>0.45–2.85</td>
<td>0.55–2.95</td>
</tr>
<tr>
<td></td>
<td>Mean</td>
<td>38.4</td>
<td>31.0</td>
<td>146.5</td>
<td>159.6</td>
<td>68.9</td>
<td>1.32</td>
<td>1.51</td>
</tr>
<tr>
<td></td>
<td>SD</td>
<td>9.2</td>
<td>6.2</td>
<td>9.0</td>
<td>17.3</td>
<td>25.7</td>
<td>0.62</td>
<td>0.65</td>
</tr>
</tbody>
</table>

Fig 1  Circuit diagram of equipment used to measure ventilation and gas exchange.
graphs. The $V_E$ and HR responses were expressed as maximal values ($V_E \text{ max}$; HR max) and at interpolated values of $V_O_2$ of 0·75I, 1·0I, and 1·5I ($V_E^{0.75}$, $V_E^{1.0}$, $V_E^{1.5}$; HR$^{0.75}$, HR$^{1.0}$, HR$^{1.5}$) (Cotes, 1969; Spiro et al, 1974). The pattern of breathing was assessed by plotting $V_E$ against $V_T$, as recommended by Hey et al (1966). These authors found that the relationship could be described as $V_E = m (V_T - k)$ l/min where m has the units of frequency and k of volume.

Submaximal tidal volumes have been expressed as the slope $V_E/V_T$ (m) and as tidal volumes at $V_E$ of 20 and 30 l/min ($V_{20}$, $V_{30}$).

Results

MAXIMAL OXYGEN UPTAKE ($V_O_2 \text{ max}$)

$V_O_2$ max ranged from 11·0 to 34·1 ml/min/kg body weight (n=20, mean =24·8, SD =6·6). For the men it ranged from 11·0 to 33·7 ml/min/kg body weight (n=9, mean=25·7, SD =6·0, SEM =2·0) and for the women from 13·2 to 34·1 ml/min/kg body weight (n=11, mean=24·3, SD =5·9, SEM =1·8). Both these values are statistically significantly lower ($p < 0·01$) than an age-matched group of normal controls (Bruce et al, 1973).

MAXIMAL EXERCISE VENTILATION ($V_E \text{ max}$)

Sixteen subjects were forced to stop exercising by ventilatory factors. $V_E$ max ranged from 13·13 to 76·05 l/min (n=16, mean =36·41, SD =17·73). The ratio of $V_E$ max to the MVV (ie the dyspnoeic index) was 0·70 (n=16, SD =0·14). The difference between those with paralytic scoliosis (n=6, mean =0·62, SEM =0·04) and the non-paralytic (n=10, mean =0·74, SEM =0·05) was not significant.

MINUTE VENTILATION ($V_E$)

The response of the minute ventilation ($V_E$) during exercise is displayed in table 2. The subjects have been subdivided according to their age and sex for comparison with Spiro's (1975) normal values. $V_E^{0.75}$, 1·0I, 1·5I were all significantly greater ($p < 0·05$) in the women than in the men, although there was no appreciable difference in slope $V_E/V_O_2$ between the sexes.

In both sexes $V_E^{0.75}$, 1·0I, 1·5I were significantly greater than normal (Spiro, 1975) ($p < 0·05$ for $V_E^{0.75}$, 1·0I in men; $p < 0·01$ for $V_E^{0.75}$, 1·0I in women and $V_E^{1.5}$ in both sexes). All the values were about 20% greater than normal. Slope $V_E/V_O_2$ did not differ from normal.

PATTERN OF VENTILATION

The tidal volume increased linearly with $V_E$ in each patient until $V_T$ max was reached. The response of $V_T$ was expressed by the method of Hey et al (1966) (fig 2). All 26 patients were used in this plot. For the men and women aged 20–39 years the differences between k, m, VC, $V_{30}$, $V_{30}/VC \times 100\%$, $V_T$ max, and $V_T$ max/VC $\times 100\%$ were not significant. The differences in m, $V_{30}$, and $V_{30}/VC \times 100\%$ were significant ($p < 0·05$) (table 3).

The results show interesting differences from the normal subjects of Spiro et al (1974) (fig 2). The intercept on the x axis, k, is smaller than normal ($p < 0·05$ for men; $p < 0·01$ for women), but the slope of $V_E/V_T$ (m) is greater than normal ($p < 0·05$ for men; $p < 0·01$ for women). $V_{30}$, $V_{30}$, and $V_T$ max are all below normal in both sexes ($p < 0·01$).

![Fig 2 Relationship between $V_E$ and tidal volume in all 26 scoliotic patients and normal subjects (Spiro, 1975), calculated from mean slopes, intercepts, and maximal tidal volumes.](http://thorax.bmj.com/content/33/4/457)

Table 2  Response of ventilation during increasing work rate test

<table>
<thead>
<tr>
<th>Index</th>
<th>Group</th>
<th>n</th>
<th>Mean</th>
<th>SD</th>
</tr>
</thead>
<tbody>
<tr>
<td>$V_E/V_O_2$</td>
<td>Men, 20–39 years</td>
<td>7</td>
<td>27·4</td>
<td>4·2</td>
</tr>
<tr>
<td></td>
<td>Men, &gt; 20 years</td>
<td>10</td>
<td>28·1</td>
<td>4·2</td>
</tr>
<tr>
<td></td>
<td>Women, 20–39 years</td>
<td>12</td>
<td>30·3</td>
<td>6·0</td>
</tr>
<tr>
<td>$V_{E,T}$ (l/min)</td>
<td>Men, 20–39 years</td>
<td>6</td>
<td>21·1</td>
<td>2·1</td>
</tr>
<tr>
<td></td>
<td>Men, &gt; 20 years</td>
<td>9</td>
<td>21·2</td>
<td>2·2</td>
</tr>
<tr>
<td></td>
<td>Women, 20–39 years</td>
<td>9</td>
<td>23·1</td>
<td>2·4</td>
</tr>
<tr>
<td>$V_{E,O}$ (l/min)</td>
<td>Men, 20–39 years</td>
<td>5</td>
<td>27·8</td>
<td>3·1</td>
</tr>
<tr>
<td></td>
<td>Men, &gt; 20 years</td>
<td>7</td>
<td>27·5</td>
<td>2·6</td>
</tr>
<tr>
<td></td>
<td>Women, 20–39 years</td>
<td>8</td>
<td>31·1</td>
<td>3·8</td>
</tr>
<tr>
<td>$V_{E,T}$ (l/min)</td>
<td>Men, 20–39 years</td>
<td>2</td>
<td>41·8</td>
<td>1·1</td>
</tr>
<tr>
<td></td>
<td>Men, &gt; 20 years</td>
<td>3</td>
<td>42·7</td>
<td>1·8</td>
</tr>
<tr>
<td></td>
<td>Women, 20–39 years</td>
<td>1</td>
<td>53·1</td>
<td>—</td>
</tr>
</tbody>
</table>
When these results are corrected for the small VC of these scoliotic subjects the abnormalities are reversed (fig 3). The values for VC are below normal (p < 0.01 for men; p < 0.05 for women), and VT20/VC and VT20/VC are above normal (p < 0.01 for both sexes). VT max/VC, however, is within the normal range in both sexes.

HEART RATE
The response of the heart rate in both sexes during the increasing work rate test is displayed in table 4. The heart rate was significantly faster (p < 0.01) in women than men at Vo2 0.75, 1.0, 1.5 I/min. However, the difference in slope HR/Vo2 between the women and men aged 20–39 years was not significant.

HR0.75, 1.0, 1.5 and slope HR/Vo2 were significantly greater (p < 0.01) in both sexes than in normal subjects (Spiro, 1975) except for HR1.5 in women and slope HR/Vo2 in men over 40. However, these groups contained only two and three subjects respectively. In the 20 who achieved maximal exercise, heart rate ranged from 128 to 201 beats min⁻¹ (mean 168).

ARTERIAL BLOOD GASES
The Po2 at rest ranged from 38.0 to 100.5 mmHg (n = 11, mean = 73.8, SD = 16.7). The Paco2 at rest ranged from 30.9 to 87.7 mmHg (n = 11, mean = 48.3, SD = 15.9). The changes after exercise were not statistically significant for either Po2 or Paco2.

Discussion
The results in those with scoliosis show several definite differences from normal. Firstly, Vo2 max was significantly less than normal (p < 0.01) for both sexes, even when corrected for total body weight. In 16 of the 20 subjects who exercised maximally (six stopped prematurely due to tiredness) exercise was limited by their ventilation. This contrasts with
normal subjects whose exercise capacity is circulation-limited. It does however explain why $V_O_2\text{ max}$ was linearly related in those with scoliosis to two estimates of maximal ventilation, $FEV_1$ and $VE\text{ max}$ (fig 4). While this does not hold for normal subjects, similar equations have been obtained in chronic bronchitics, whose exercise is also ventilation-limited (Spiro et al, 1975). In the subjects of the present study the prediction formulae for $V_O_2\text{ max}$ were

$$V_O_2\text{ max} = 0.53\ FEV_1 + 0.365\ l/min$$

(n = 20, r = 0.932, p < 0.001)

$$= 0.024\ VE\text{ max} + 0.199\ l/min$$

(n = 20, r = 0.953, p < 0.001)

$VE\text{ max}$ was a normal proportion (70%) of the MVV (ie the dyspnoeic index was normal), but in absolute terms it was greatly reduced. For the men the mean $VE\text{ max}$ was only 41.96 l/min, which is 35.2% normal (Cotes et al, 1969). In the women it was 32.09 l/min, which is 40.4% normal (Cotes et al, 1969). $VE\text{ max}$ was linearly related to $FEV_1$, $VC$, and $MVV$ by the following equations (fig 5)

$$VE\text{ max} = 21.8\ FEV_1 + 8.7\ l/min$$

(n = 16, r = 0.921, p < 0.001)

$$= 21.4\ VC + 6.2\ l/min$$

(n = 16, r = 0.931, p < 0.001)

$$= 0.46\ MVV + 10.0\ l/min$$

(n = 16, r = 0.951, p < 0.001)
A similar relationship, but with a larger intercept, was obtained for chronic bronchitics by Spiro et al (1975).

Although the gross diminution in \( Ve \) max is the main cause of the abnormally low \( \dot{V}O_2 \) max, the minute ventilation for any given \( \dot{V}O_2 \) was also significantly greater than normal. Thus not only was the upper limit of minute ventilation decreased, but the subjects hyperventilated relative to their work rate as well. There was no correlation between slope \( Ve/\dot{V}O_2 \) and the angle of scoliosis, VC, PaO2, PaCO2, or pH before or after exercise or to the change in any of these during exercise. The extra work expended in hyperventilating with a stiff deformed thorax decreases the amount of energy available for performing external work.

The tidal volume increased linearly with ventilation until \( V_T \) max was reached. Increase in ventilation beyond this point was accomplished by an increase in respiratory frequency. This is the normal pattern (Hey et al, 1966). The slope \( Ve/V_T \) (m) was greater in those with scoliosis than normal, and this is also reflected in the small values for the tidal volume at minute ventilations of 20 and 30 l/min. If the tidal volumes are corrected for the small vital capacities of these subjects, however, \( n \) becomes less than normal and \( V_{T20}/VC \) and \( V_{T30}/VC \) are above normal. Thus although in absolute volumes the \( V_T \) of those with scoliosis is less than normal at any given minute ventilation, it is actually a larger percentage of their vital capacity than is normal. They are partially compensating for their small VC by using a greater proportion of it in tidal breathing at any given \( Ve \). Their maximal tidal volumes are also small, although \( V_T \) max/VC was normal.

Almost all the indices of the heart rate response to exercise are significantly above Spiro’s (1975) normal ranges. Cotes et al (1973), however, have shown that the tachycardia of exercise is inversely proportional to the fat free mass (FFM):

\[
\text{slope } HR/\dot{V}O_2 = 2580 \text{ FFM}^{-1} + 1585 \text{ beats/min}
\]

\[(\text{coefficient of variation} = 11.8\%)\]

where FFM is expressed in kg.

The mean FFM of those with scoliosis was only 36.4 kg (SD 9.6 kg). This correction is therefore quantitatively important. If it is applied to the non-paralytic subjects the observed/predicted slope HR/\( \dot{V}O_2 \) is 1.02 (n = 17, SEM = 0.08) but for those with scoliosis with neurological or muscular diseases it is 1.38 (n = 9, SEM = 0.12). In the former group the tachycardia is not abnormal but is a physiological consequence of their small size. The tachycardia in the subjects with neurological or muscular disease remains unexplained. It may be an artefact since Cotes’s correction formula depends on a normal muscle:bone ratio and these patients, especially those who have had poliomyelitis, probably have less muscle than normal. If this is so it would invalidate the use of this formula for these patients and could explain the apparent tachycardia.

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References


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