Pulmonary restrictive effect of bracing in mild idiopathic scoliosis

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ABSTRACT The use of bracing in the treatment of mild idiopathic scoliosis is controversial. A study of 33 adolescents showed that bracing significantly decreased lung volumes. Functional residual capacity was reduced by a mean of 26%, 18% of children showing a reduction of greater than 40%. The mean reduction in total lung capacity was 16% and in forced vital capacity 18%. This restriction of lung function by bracing might have a deleterious effect on lung growth or might impose an additional risk factor in the presence of other disorders, such as asthma and diaphragmatic weakness. The use of bracing in individuals with mild scoliosis should be judiciously reassessed.

Scoliosis is one of man's earliest known physical deformities. It has been depicted in cave drawings, noted in the mummified remains of the pharaohs, and aroused fear in Victor Hugo's tale of Quasimodo, the Hunchback of Notre Dame.

Despite this long history, its treatment, particularly bracing, remains controversial. The use of bracing in the management of scoliosis began during the 1940s with the introduction of the Milwaukee brace, designed to stabilise the spine postoperatively.¹ During the 1950s and 1960s bracing began to be used in the non-operative management of scoliosis. During the 1970s the Boston brace was introduced.² There is continuing debate in orthopaedic publications about the indications and effectiveness of bracing programmes.^{3,4}

Although braces have been used extensively in the past 30 years, their effect on underlying lung function and chest wall mechanics is largely unknown. We report the effect of bracing on lung volumes in 33 adolescents with idiopathic scoliosis.

Patients and methods

We studied 33 adolescents, six male and 27 female, with idiopathic thoracic scoliosis attending an orthopaedic clinic and being treated by bracing. Eight used a Milwaukee brace and 25 a Boston brace. Their mean

age was 13.3 years and the mean thoracic Cobb angle 29°. In five children the thoracic curve had improved with bracing and at the time of testing was less than 20 degrees. The mean age of onset was 11.7 years (range 6-16 years) and the mean duration of bracing 1.4 years (range 1 month-5 years). None of the patients had cardiopulmonary symptoms at the time of testing. Functional residual capacity (FRC) and total lung capacity (TLC) were measured in the sitting position by means of body plethysmography (Jaeger Body-screen 2) both with and without the brace. The order of testing—that is, whether the brace was on or off for the first measurements—was randomly selected to allow for a learning effect. All spirometric volumes were corrected to BTPS. The non-deformed height was taken as equal to arm span. In our laboratory the arm-span:height ratio estimated from 2368 measurements of 8-18 year old subjects is close to unity (0.999 (SD 0.023) for girls and 1.006 (0.022) for boys).

The Milwaukee brace reduces lumbar lordosis with a polypropylene pelvic girdle and attempts to correct the thoracic curve with a metal vertical suprastructure on which are mounted pressure pads. The Boston bracing system also uses a polypropylene girdle, which, unlike the former, extends to enclose the lower thorax, again attempting to correct the spinal curve by means of pressure pads mounted on the inner surface, acting on the apices of the curve.

Six children with a brace induced reduction in FRC of over 30% were further studied to assess the effect of bracing on oxygen saturation during sleep. Oxygen saturation was monitored overnight with a Nelcor pulse oximeter; studies were performed on two nights, one with and the other without the brace.

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We used analysis of variance, repeated measures design,⁵ to assess the effect of gender and brace type on reduction in lung volumes; *p* values of less than 0.05 were regarded as significant.

The study was approved by the hospital ethics committee and informed consent was obtained from subjects and parents.

Results

As a group, the subjects had normal lung volumes when unbraced (table 1). Although some patients had a mild restrictive defect, this did not correlate with age of onset of scoliosis or duration of bracing.

With the brace on, there were significant reductions in all the subdivisions of total lung capacity, especially FRC (*p* < 0.001). FVC and FEV₁ were also reduced (*p* < 0.001) (table 2). The 95th centiles for coefficient of variation for lung volumes in normal subjects from our laboratory are included in the table for comparison. The mean reduction in FRC was 26%. Six children (18%), however, had a reduction of over 40% and 13 children (39%) had a reduction of at least 30%. No difference was found between the restrictive effect of the brace on boys and on girls. There was also no difference between the restrictive effects on lung volumes of the Boston and the Milwaukee brace.

Table 1 Details of subjects and their lung function while unbraced

	Male	Female
Number	6	27
Age (y)*	12.4 (11.0–15.0)	13.8 (10.0–17.0)
Arm span (cm)*	154 (132–184)	164 (140–178)
Thoracic Cobb angle (°)*	32 (20–40)	28 (10–44)
Age at onset (y)*	8 (6–13)	13 (7–16)
Duration of bracing (y)*	3.3 (0.7–5)	0.9 (0.1–3.8)
Lung function (% predicted)†		
VC	87 (10)	88 (13)
FEV ₁	82 (10)	86 (13)
FRC	97 (18)	103 (17)
TLC	93 (9)	99 (12)

*Median and range.

†Mean and standard deviation.

VC—vital capacity; FEV₁—forced expiratory volume in one second; FRC—functional residual capacity; TLC—total lung capacity.

Table 2 Effects of bracing on lung volumes (in litres; means with standard deviations)

	Brace on	Brace off	Mean change (%)	95th centile coefficient of variation (%)
FVC	2.3 (0.6)	2.8 (0.6)	17.8*	3.9
FEV ₁	2.0 (0.5)	2.4 (0.5)	16.7*	5.2
FRC	1.7 (0.5)	2.3 (0.5)	26.0*	9.8
TLC	3.5 (0.7)	4.2 (0.7)	16.7*	5.2

**p* = < 0.001.

FVC—forced vital capacity; other abbreviations as in table 1.

All overnight oximetry studies, both with and without the brace, showed normal oxygen saturation levels of 97–100% during sleep.

Discussion

The use of braces in the conservative management of idiopathic scoliosis has been widely practised for the past four decades. Latterly their role has been under critical review. Recent long term reviews of both Milwaukee and Boston braces concluded that the mean effect of orthotic treatment is to produce a curve which is only a few degrees better than the original.^{6–8}

The effect of these restrictive braces on the underlying lung and chest wall has remained unrecognised. Sevastikoglou *et al*⁹ studied the effect of the Milwaukee brace in 26 patients with idiopathic scoliosis and reported that the brace did not alter vital capacity significantly, a conclusion with which we disagree. No previous study has examined in detail the change in the subdivisions of total lung capacity associated with bracing.

In our patients there were significant reductions in FEV₁ and FVC and in all the subdivisions of TLC especially FRC (table 2). The reduction in lung volumes appears to be due to a combination of factors. In an attempt to reduce lumbar lordosis the brace is fitted tightly around the abdomen, thus displacing abdominal contents into the chest, reducing lung volumes, and restricting the downward movement of the diaphragm. With the Boston brace there is also direct pressure effect on the ribcage, which further restricts respiratory excursion.

It is important to note that there was no difference in the degree of restriction of lung volumes imposed by the two types of brace. Although the Boston brace may vary from centre to centre, depending on individual modification, the Milwaukee brace design is consistent between centres, suggesting that the restrictive effect of these braces is not due to local design practices.

During inspiration, with descent of the diaphragm the intra-abdominal pressure rises. This pressure is relieved by the outward movement of the abdominal wall and lower rib cage. If these movements are restricted by a brace the intra-abdominal pressure will rise and impose an additional load on the diaphragm which might have important implications for a child with diaphragmatic weakness.

Normal subjects have a 20% reduction in FRC on changing from the sitting to the supine posture.¹¹ As the mean reduction in FRC for children sitting with brace on was 26% we were concerned that there might be an additional effect while the child slept. This could be a particular problem during REM sleep, when there

may be a further fall in FRC owing to relaxation of the intercostal muscles,¹² and thus a risk of oxygen desaturation. Overnight oxygen saturation was, however, normal in all the six children whose brace restriction was the most severe.

The effects we have found might also have implications for a child who has asthma in addition. During an attack of asthma expiratory flows at all lung volumes are reduced. This is partially offset by an increase in FRC,¹³ achieved by braking expiratory flow with partial glottis closure, increasing the respiratory rate and persisting inspiratory muscle activity during expiration.^{14,15} The restrictive effect of a brace would be likely to limit the child's ability to increase FRC and to breathe at higher lung volumes.

An effect of scoliosis on lung growth has been documented¹⁶ but the effect of prolonged use of a restricting brace during a period of continuing alveolar growth is unknown.

Although there is general agreement that bracing may be effective in progressive curves of 30–40°, idiopathic scoliosis beginning after the age of 11 years does not appear to carry the risk of cardiorespiratory failure that was hitherto believed.¹⁷ Thus if braces do not appreciably alter the natural history of adolescent curves,³ their use needs to be judiciously reassessed because, as we have shown, they can have a considerable effect on lung volumes, and there may be a potential risk of impairing lung growth or aggravating underlying disorders such as asthma or diaphragmatic weakness.

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